# **Encoding Time-Series Explanations through Self-Supervised Model Behavior Consistency**

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#### Abstract

Interpreting time series models is uniquely challenging because it requires identifying both the location of time series signals that drive model predictions and their matching to an interpretable temporal pattern. While explainers from other modalities can be applied to time series, their inductive biases do not transfer well to the inherently uninterpretable nature of time series. We present TIMEX, a time series consistency model for training explainers. TIMEX trains an interpretable surrogate to mimic the behavior of a pretrained time series model. It addresses the issue of model faithfulness by introducing model behavior consistency, a novel formulation that preserves relations in the latent space induced by the pretrained model with relations in the latent space induced by TIMEX. TIMEX provides discrete attribution maps and, unlike existing interpretability methods, it learns a latent space of explanations that can be used in various ways, such as to provide landmarks to visually aggregate similar explanations and easily recognize temporal patterns. We evaluate TIMEX on 8 synthetic and real-world datasets and compare its performance against state-of-the-art interpretability methods. We also conduct case studies using physiological time series. Quantitative evaluations demonstrate that TIMEX achieves the highest or second-highest performance in every metric compared to baselines across all datasets. Through case studies, we show that the novel components of TIMEX show potential for training faithful, interpretable models that capture the behavior of pretrained time series models.

# 1 Introduction

State-of-the-art time series models are high-capacity pre-trained neural networks [1, 2] often seen as black boxes due to their internal complexity and lack of interpretability [3]. However, practical use requires techniques for auditing and interrogating these models to rationalize their predictions. Interpreting time series models poses a distinct set of challenges due to the need to achieve two goals: pinpointing the specific *location* of time series signals that influence the model's predictions, and aligning those signals with *interpretable temporal patterns* [4]. Applying explainers designed for other types of data is difficult, as their inductive biases struggle to adapt to the inherently uninterpretable

nature of time series. The dynamic nature and multi-scale dependencies within time series data require temporal interpretability techniques.

Research in model understanding and interpretability developed *post-hoc* explainers that treat pretrained models as black boxes and do not need access to internal model parameters, activations, and gradients. Recent research, however, shows that such post hoc methods suffer from a lack of faithfulness and stability, among other issues [5, 6, 7]. A model can also be understood by investigating what parts of the input it attends to through attention mapping [8, 9, 10] and measuring the impact of modifying individual computational steps within a model [11, 12]. Another major line of inquiry investigates internal mechanisms by asking what information the model contains [13, 14, 15]. For example, it has been found that even when a language model is conditioned to output falsehoods, it may include a hidden state that represents the true answer internally [16]. Such a gap between external failure modes and internal states can only be identified by probing model internals. Such representation probing has been used to characterize the behaviors of language models, but leveraging these strategies to understand time series models has yet to be attempted. These lines of inquiry drive the development of *in-hoc* explainers [17, 18, 19, 20, 21, 22] that build inherent interpretability into the model through architectural modifications [18, 19, 23, 20, 21] or regularization [17, 22]. However, no *in-hoc* explainers have been developed for time series data. While explainers designed for other modalities can be adapted to time series, their inherent biases do not translate effectively to the uninterpretable nature of time series data and can miss important structures in time series.

Explaining time series models is challenging for many reasons. First, large time series data are not visually interpretable, as opposed to imaging or text datasets. Next, time series often exhibit dense informative features, in contrast to more explored modalities such as imaging, where informative features are often sparse. In time series datasets, timestep-to-timestep transitions can be negligible and temporal patterns only show up when looking at time segments and long-term trends. In contrast, in text datasets, word-to-word transitions are informative for language modeling and understanding. Further, time series interpretability involves understanding dynamics of the model and identifying trends or patterns. Another key issue with applying prior methods is that they treat all *time steps* as separate features, ignoring potential time dependencies and contextual information; we need explanations that are *temporally connected* and visually digestible. While understanding predic-



Figure 1: TIMEX learns a latent space of explanations along with landmarks to summarize groups of informative temporal patterns in time series.

tions of individual samples is valuable, the ability to establish *connections between explanations of various samples* (for example, in an appropriate latent space) could help alleviate these challenges.

**Present work.** We present TIMEX, a novel time series *in-hoc* explainer that produces interpretable attribution masks as explanations over time series inputs (Figure 1). Our codebase is at https: //github.com/mims-harvard/TimeX. ① A key contribution of TIMEX is the introduction of *model behavior consistency*, a novel formulation that ensures the preservation of relationships in the latent space induced by the pretrained model, as well as the latent space induced by TIMEX. ② In addition to achieving model behavior consistency, TIMEX offers interpretable attribution maps, which are valuable tools for interpreting the model's predictions, generated using discrete straight-through estimators (STEs), a type of gradient estimators that enable end-to-end training of TIMEX models. ③ Unlike existing interpretability methods, TIMEX goes a step further by learning a latent space of explanations. By incorporating model behavior consistency and leveraging a latent space of similar explanations and the recognition of temporal patterns. ④ We test our approach on 8 synthetic and real-world time series datasets, including datasets with carefully processed ground-truth explanations to quantitatively benchmark it and compare it to general explainers, state-of-the-art time series explainers, and *in-hoc* explainers.



# 2 Related work

**Model understanding and interpretability.** As neural networks have grown, so has the need to help users interpret a network's behavior. The vast majority of explainable AI research [24] has focused on natural language processing (NLP) [25, 26, 27] and computer vision (CV) [28, 29, 30]. Commonly used techniques, such as Integrated Gradients [31] and Shapley Additive Explanations (SHAP) [3], and their variants have originated from these domains and gained popularity. XAI has gained significant interest in NLP and CV due to the inherent interpretability of their data. However, this familiarity can introduce confirmation bias [32]. Recent works have expanded to other data modalities, including graphs [33, 6] and time series [34, 35], as outlined below.

The literature primarily focuses on *post-hoc* explainability, where explanations are provided for a trained and frozen model's behavior [36, 37]. However, saliency maps, a popular approach [38, 31, 39], have pitfalls when generated *post-hoc*: they are surprisingly fragile [5], and lack sensitivity to their explained models [40]. Surrogate-based approaches have also been proposed [41, 42, 43], but these simplified surrogate models fall short compared to the original predictor they aim to explain.

Unlike *post-hoc* explainability, *in-hoc* methods aim for inherently interpretable models. This can be accomplished by modifying the model's architecture [20], training procedure using jointly-trained explainers [44], adversarial training [45, 46, 47], regularization techniques [17, 22], or refactoring the latent space [48, 49]. However, such models often struggle to achieve state-of-the-art predictive performance, and to date, these methods have seen limited use for time series.

**Beyond instance-based explanations.** Several methods have been proposed to provide users with information beyond a single, instance-based saliency map. Prototype models strive to offer a representative sample or region in the latent space [50, 51]. Such methods are inherently interpretable, as predictions are directly tied to patterns in the feature space. Further, explainability through human-interpretable exemplars has been gaining popularity. Concept-based methods decompose model predictions into human-interpretable *concepts*. Many works rely on annotated datasets with hand-picked concepts (*e.g.*, "stripes" in an image of a zebra). Relying on access to a-priori defined concepts, concept bottleneck models learn a layer that attributes each neuron to one concept [23]. This limitation has spurred research in concept discovery by composing existing concepts [52, 53] or grounding detected objects to natural language [54]. However, the computer vision focus of these works poses limited transfer to other domains like time series.

**Time series explainability.** In contrast to other modalities, time series often have multiple variables, and their discriminative information is spread over many timesteps. Building on these challenges, recent works have begun exploring XAI for time series [55, 56, 57, 58, 59, 60, 34, 61]. Many methods modify saliency maps [35, 62, 57] or surrogate methods [58, 63] to work with time series data. Two representative methods are WinIT [64] and Dynamask [57]. WinIT learns saliency maps with temporal feature importances, while Dynamask regularizes saliency maps to include temporal smoothing. However, these methods rely on perturbing timesteps [62], causing them to suffer from a lack of faithfulness. Common perturbation choices in CV, like masking with zeros, make less sense for time series [55]. Perturbed time series may be out-of-distribution for the model due to shifts in shape [65], resulting in unfaithful explanations akin to adversarial perturbation [66].

#### 3 **Problem formulation**

**Notation.** Given is a time series dataset  $\mathcal{D} = (\mathcal{X}, \mathcal{Y}) = \{(\mathbf{x}_i, y_i) | i = 1, ..., N\}$  where  $\mathbf{x}_i$  are input samples and  $y_i$  are labels associated to each sample. Each sample  $\mathbf{x}_i \in \mathbb{R}^{T \times d}$  is said to have T time steps and d sensors. A *feature* is defined as a time-sensor pair, where the time t and sensor kfor input  $\mathbf{x}_i$  is  $\mathbf{x}_i[t, k]$ . Without loss of generality, our model is defined for univariate (d = 1) and multivariate (d > 1) settings. Each  $y_i \in \{1, 2, ..., C\}$  belongs to one of C classes. A classifier model consists of an encoder G and predictor  $\overline{F}$ . The encoder G produces an embedding of input  $\mathbf{x}_i$ , *i.e.*,  $G(\mathbf{x}_i) = \mathbf{z}_i \in \mathbb{R}^{d_z}$ , while the predictor produces some prediction from the embedding in the form of a logit, *i.e.*,  $F(G(\mathbf{x}_i)) = \hat{y}_i \in [0, 1]^C$  where  $\operatorname{argmax}_j \hat{y}_i[j] \in \{1, ..., C\}$  is the predicted label. The latent space induced by G is defined as Z, e.g.,  $G: \mathcal{X} \to Z$ . We will refer to  $F(G(\cdot))$  as the reference model while G is the reference encoder and F is the reference predictor. An explanation is defined as a continuous map of the features that conveys the relative importance of each feature for the prediction. The explanation for sample  $\mathbf{x}_i$  is given as  $E(\mathbf{x}_i) \in \mathbb{R}^{T \times d}$  where for any times  $t_1, t_2$ and sensors  $k_1, k_2, E(\mathbf{x}_i[t_1, k_1]) > E(\mathbf{x}_i[t_2, k_2])$  implies that  $\mathbf{x}_i[t_1, k_1]$  is a more important feature for the task than  $\mathbf{x}_i[t_2, k_2]$ .

#### 3.1 **TIMEX problem formulation**

TIMEX creates an inherently-interpretable surrogate model for pretrained time series models. The surrogate model produces explanations by optimizing two main objectives: interpretability and faithfulness to model behavior. First, we generate interpretable explanations via an attribution map  $E(\mathbf{x}_i)$  that identifies succinct, connected regions of input that are important for the prediction. To ensure faithfulness to the reference model, we introduce a novel objective for training TIMEX: model behavior consistency (MBC). With MBC, a TIMEX model learns to mimic internal layers and predictions of the reference model, yielding a time series a high-fidelity explainer. MBC is defined as:

**Definition 3.1** (Model Behavior Consistency (MBC)). The explanations E and explanation encoder  $G^E$  are consistent with the pretrained model G and predictor F on dataset  $\mathcal{D}$  if the following two requirements are satisfied:

- [Consistent reference encoder]: Relationship between z<sub>i</sub> = G(x<sub>i</sub>) and z<sub>j</sub> = G(x<sub>j</sub>) in the space of reference encoder is preserved by the explainer, z<sub>i</sub><sup>E</sup> = G<sup>E</sup>(E(x<sub>i</sub>)) and z<sub>j</sub><sup>E</sup> = G<sup>E</sup>(E(x<sub>j</sub>)), such that: D<sub>Z</sub>(z<sub>i</sub>, z<sub>j</sub>) ≃ D<sub>Z</sub><sup>E</sup>(z<sub>i</sub><sup>E</sup>, z<sub>j</sub><sup>E</sup>) for samples x<sub>i</sub>, x<sub>j</sub> ∈ D.
  [Consistent reference predictor]: Relationship between reference predictor ŷ<sub>i</sub> = F(z<sub>i</sub>) and latent explanation predictor ŷ<sub>i</sub><sup>E</sup> = F(z<sub>i</sub><sup>E</sup>) is preserved, ŷ<sub>i</sub> ≃ ŷ<sub>i</sub><sup>E</sup> for every sample x<sub>i</sub> ∈ D.

Our central problem formulation is defined as realizing the MBC between a reference model and an interpretable TIMEX model:

**Problem statement 3.1** (TIMEX). Given are pretrained time series encoder G and predictor F that are trained on a time series dataset  $\mathcal{D}$ . TIMEX provides explanations  $E(\mathbf{x}_i)$  for every sample  $\mathbf{x}_i \in \mathcal{D}$ in the form of interpretable attribution maps. These explanations satisfy *model behavior consistency* through the latent representation space of explanations  $Z^E$  generated by the explanation encoder  $G^E$ .

TIMEX is designed to counter several challenges in interpreting time series models. First, TIMEX avoids the pitfall known as the occlusion problem [67]. Occlusion occurs when some features in an input  $x_i$  are perturbed in an effort that the predictor forgets those features. Since it is well-known that occlusion can produce out-of-distribution samples [68], this can cause unpredictable shifts in the behavior of a fixed, pretrained model [69, 70, 71]. In contrast, TIMEX avoids directly masking input samples to G. First, TIMEX trains an interpretable surrogate  $G^E$  to match the behavior of G. Second, MBC is designed to improve the faithfulness of TIMEX to G. By learning to mimic multiple states of  $F(G(\cdot))$  using the MBC objective, TIMEX learns highly-faithful explanations, unlike many post-hoc explainers that provide no explicit optimization of faithfulness. Finally, TIMEX's explanations are driven by learning a latent explanation space, offering richer interpretability data.

#### 4 **TIMEX** method

We now present TIMEX, an approach to train an interpretable surrogate model to provide explanations for a pretrained time series model. TIMEX learns explanations through a consistency learning objective where an explanation generator  $H^E$  and explanation encoder  $G^E$  are trained to match

intermediate feature spaces and the predicted label space. We will break down TIMEX in the following sections by components:  $H^E$ , the explanation generator,  $G^E$ , the explanation encoder, and the training objective of  $G^E(H^E(\cdot))$ , followed by a discussion of practical considerations of TIMEX. An overview of TIMEX is depicted in Figure 2.

#### 4.1 Explanation generation

Generating an explanation involves producing a mask  $M_{\mathcal{X}}$  where if  $M_{\mathcal{X}}[t_1, k_1] > M_{\mathcal{X}}[t_2, k_2]$ , then  $M_{\mathcal{X}}[t_1, k_1]$  is considered as more important for the prediction than  $M_{\mathcal{X}}[t_2, k_2]$ . Explanation generation is performed through an explanation generator  $H^E : \mathcal{X} \to \mathbf{p} \in [0, 1]^{T \times d}$ . We learn  $\mathbf{p}$ based on a procedure proposed by [49], but we adapt their procedure for time series. Intuitively,  $\mathbf{p}$ parameterizes a Bernoulli at each time-sensor pair, and the mask  $M_{\mathcal{X}}$  is sampled from this Bernoulli distribution during training, *i.e.*,  $M_{\mathcal{X}} \sim \mathbb{P}_{\mathbf{p}}(M_{\mathcal{X}}|\mathcal{X}) = \prod_{t,k} \text{Bern}(\mathbf{p}_{t,k})$ . This parameterization is directly interpretable as attribution scores: a low  $\mathbf{p}_{t,k}$  means that time-sensor pair (t, k) has a low probability of being masked-in. Thus,  $\mathbf{p}$  is also the explanation for  $\mathbf{x}_i$ , *i.e.*,  $E(\mathbf{x}) = \mathbf{p}$ .

The generation of **p** is regularized through a divergence with Bernoulli distributions Bern(r), where r is a user-chosen hyperparameter. Denote the desired distribution of **p** as  $\mathbb{Q}(M_{\mathcal{X}}) = \prod_{(t,k)} \text{Bern}(r)$ . Then the objective becomes:

$$\mathcal{L}_m(\mathbf{p}) = \mathbb{E}[D_{\mathrm{KL}}(\mathbb{P}_{\mathbf{p}}(M_{\mathcal{X}}|\mathcal{X})||\mathbb{Q}(M_{\mathcal{X}}))] = \sum_{t,k} \mathbf{p}_{t,k} \log \frac{\mathbf{p}_{t,k}}{r} + (1 - \mathbf{p}_{t,k}) \log \frac{1 - \mathbf{p}_{t,k}}{1 - r} \quad (1)$$

The sampling of  $M_{\mathcal{X}} \sim \mathbb{P}_{\mathbf{p}}(M_{\mathcal{X}}|\mathcal{X})$  is performed via the Gumbel-Softmax trick [72, 73], which is a differentiable approximation of categorical sampling. Importantly,  $M_{\mathcal{X}}$  is stochastically generated, which as discussed in [49, 74], regularizes the model to learn robust explanations.

To generate interpretable attribution masks, TIMEX optimizes for the connectedness of predicted distributions:

$$\mathcal{L}_{\rm con}(\mathbf{p}) = \frac{1}{T \times d} \sum_{k=1}^{d} \sum_{t=1}^{T-1} \sqrt{(\mathbf{p}_{t,k} - \mathbf{p}_{t+1,k})^2}.$$
 (2)

The generator of explanations  $H^E$  learns directly on input time series samples  $\mathcal{X}$  to return **p**. We build a transformer encoder-decoder structure for  $H^E$ , using an autoregressive transformer decoder and a sigmoid activation to output probabilities for each time-sensor pair.

#### 4.2 Explanation encoding

We now describe how to embed explanations with the explanation encoder  $G^E$ . Intuitively,  $G^E$  learns on the masked distribution of  $\mathcal{X}$ , which can be denoted as  $\mathcal{X}^m$ . Motivated by the occlusion problem, we avoid directly applying the masks onto the pre-trained, frozen G, as  $\mathcal{X}^m$  and  $\mathcal{X}$  are fundamentally different distributions. Therefore, we copy the weights of G into  $G^E$  and fine-tune  $G^E$  on  $\mathcal{X}^m$ .

**Discretizing attribution masks.** When passing inputs to  $G^E$ , it is important for the end-to-end optimization to completely ignore regions identified as unimportant by  $H^E$ . Therefore, we use a straight-through estimator (STE) [72] to obtain a discrete mask  $M_{\mathcal{X}} \in \{0, 1\}^{T \times d}$ . Introduced by [75], STEs utilize a surrogate function to approximate the gradient of a non-differentiable operation used in the forward pass, such as binarization.

Applying masks to time series samples. We use two types of masking procedures: attention masking and direct-value masking. First, we employ differentiable attention masking through a multiplicative operation proposed by Nguyen et al. [76]. When attention masking does not apply, based on architecture choice or the use of multivariate inputs, we a direct-value masking procedure. We approximate a baseline distribution:  $\mathbb{B}_{\mathcal{X}} = \prod_{t,k} \mathcal{N}(\mu_{tk}, \sigma_{tk}^2)$ , where  $\mu_{tk}$  and  $\sigma_{tk}^2$  are the mean and variance over time-sensor pairs. Masking is then performed through a multiplicative replacement as:  $\mathbf{x}_i^m = (M_{\mathcal{X}} \odot \mathbf{x}_i) + (1 - M_{\mathcal{X}}) \odot b$ , where  $b \sim \mathbb{B}_{\mathcal{X}}$ .

**Justification for discrete masking.** It is important that masks  $M_{\chi}$  are discrete as opposed to continuous. Previous works have considered masking techniques [77, 48, 49] with continuous masks. However, continuous masking has a distinctly different interpretation: it applies a continuous deformation of the input towards a baseline value. While such an approach is reasonable for data modalities with discrete structures, such as sequences of tokens (as in [77, 48]) or nodes in graphs

[49], such deformation may result in a change of the shape of time series data, which is known to be important for prediction [65]. As a toy example, consider an input time series  $\mathbf{x}_i$  where the predictive pattern is driven by feature  $\mathbf{x}_i[t_1, k_1]$  being larger than all other features. If  $M_{\mathcal{X}}$  is continuous, then it is possible that for a less important feature  $\mathbf{x}_i[t_2, k_2]$ ,  $M_{\mathcal{X}}[t_1, k_1] < M_{\mathcal{X}}[t_2, k_2]$ while  $(M_{\mathcal{X}}[t_1, k_1] \odot \mathbf{x}_i[t_1, k_1]) > (M_{\mathcal{X}}[t_2, k_2] \odot \mathbf{x}_i[t_2, k_2])$ , thereby preserving the predictive pattern while the mask indicates that  $\mathbf{x}_i[t_2, k_2]$  is more important than  $\mathbf{x}_i[t_1, k_1]$ . If a surrogate model is trained on  $M_{\mathcal{X}} \odot \mathbf{x}_i$ ,  $M_{\mathcal{X}}$  may violate the ordinality expected by an attribution map as defined in Section 3. Discrete masking alleviates this issue by forcing  $M_{\mathcal{X}}$  to be binary, removing the possibility of confounds created by continuous masking. Therefore, discrete masking is necessary when learning interpretable masks on continuous time series.

#### 4.3 Model behavior consistency

The challenge lies in training  $G^E(H^E(\cdot))$  to faithfully represent  $F(G(\cdot))$ . We approach this by considering the latent spaces of G and  $G^E$ . If G considers  $\mathbf{x}_i$  and  $\mathbf{x}_j$  to be similar in Z, we expect that a faithful  $G^E$  would encode  $E(\mathbf{x}_i)$  and  $E(\mathbf{x}_j)$  similarly. However, directly aligning G and  $G^E$  is not suitable due to potential differences in the geometry of the explanation embedding space compared to the full input latent space. To address this, we introduce model behavior consistency (MBC), a novel self-supervised objective that trains the explainer model to mimic the behavior of the original model without strict alignment between the spaces. Denote the latent space induced by G and  $G^E$  as Z and  $Z^E$ , respectively. The MBC objective is thus defined as:

$$\mathcal{L}_{\text{MBC}}(Z, Z^E) = \sum_{\mathbf{z}_i, \mathbf{z}_j \in Z} \sum_{\mathbf{z}_i^E, \mathbf{z}_j^E \in Z^E} (D_Z(\mathbf{z}_i, \mathbf{z}_j) - D_{Z^E}(\mathbf{z}_i^E, \mathbf{z}_j^E))^2,$$
(3)

where  $D_Z$  and  $D_{Z^E}$  are distance functions on the reference model's latent space and the explanation encoder's latent space, respectively. This objective encourages distances to be similar across both spaces, encouraging  $Z^E$  to retain a similar local topology to Z without performing direct alignment. This is closely related to cycle-consistency loss, specifically cross-modal cycle-consistency loss as [78]. We use cosine similarity for  $D_Z$  and  $D_{Z^E}$  throughout experiments in this study, but any distance can be defined on each respective space.

In addition to MBC, we use a label consistency (LC) objective to optimize TIMEX. We train a predictor  $F^E$  on  $Z^E$  to output logits consistent with those output by F. We use a Jensen-Shannon Divergence ( $D_{JS}$ ) between the logits of both predictors:

$$\mathcal{L}_{\mathrm{LC}}(Z, Z^{E}) = \sum_{\mathbf{z}_{i}, \mathbf{z}_{j} \in \mathbb{Z}} \sum_{\mathbf{z}_{i}^{E}, \mathbf{z}_{j}^{E} \in \mathbb{Z}^{E}} \left( D_{\mathrm{JS}}(F(\mathbf{z}_{i})||F(\mathbf{z}_{j})) - D_{\mathrm{JS}}(F^{E}(\mathbf{z}_{i}^{E})||F^{E}(\mathbf{z}_{j}^{E})) \right)^{2}$$
(4)

Our total loss function on  $Z^E$  can then be defined as a combination of losses:  $\mathcal{L}_{Z^E} = \mathcal{L}_{MBC} + \lambda_{LC}\mathcal{L}_{LC}$ . **Consistency learning justification.** MBC offers three key benefits for explainability. (1) MBC enables consistency optimization across two latent spaces Z and  $Z^E$  without requiring that both  $\mathbf{x}_i$  and  $E(\mathbf{x}_i)$  be encoded by the same model, allowing the learning of E on a separate model  $F^E(G^E(\cdot)) \neq F(G(\cdot))$ . This avoids the out-of-distribution problems induced by directly masking inputs to G. (2) MBC provides a comprehensive representation of model behavior for explainer optimization. This is in contrast to perturbation explanations [38, 79, 57] which seek a labelpreserving perturbation P on  $F(G(\cdot))$  where  $F(G(P(\mathbf{x}_i))) \approx F(G(\mathbf{x}_i))$ . By using  $G(\mathbf{x}_i)$  and  $F(G(\mathbf{x}_i))$  to capture the behavior of the reference model, MBC's objective is richer than a simple label-preserving objective. (3) While MBC is stronger than label matching alone, it is more flexible than direct alignment. An alignment objective, which enforces  $\mathbf{z}_i \approx \mathbf{z}_i^E$ , inhibits  $G^E$  from learning important features of explanations not represented in Z. The nuance and novelty of MBC are in learning a latent space that is faithful to model behavior while being flexible enough to encode rich relational structure about explanations that can be exploited to learn additional features such as landmark explanations. Further discussion of the utility of MBC is in Appendix B.

#### 4.4 Learning explanation landmarks and training TIMEX models

Leveraging TIMEX's latent space, we learn landmark explanations  $\mathbf{z}^L \in \mathbb{R}^{d_z}$ . Such landmarks are desirable as they allow users to compare similar explanation patterns across samples used by the predictor. Landmarks are learned by a landmark consistency loss, and their optimization is detached

from the gradients of the explanations so as to not harm explanation quality. Denote the landmark matrix as  $\mathbf{L} \in \mathbb{R}^{n_L \times d_z}$  where  $n_L$  corresponds to the number of landmarks (a user-chosen value) and  $d_z$  is the dimensionality of  $Z^E$ . For each sample explanation embedding  $\mathbf{z}_i^E$ , we use Gumbel-Softmax STE GS to stochastically match  $\mathbf{z}_i^E$  to the nearest landmark in the embedding space. Denote the vector of similarities to each  $\mathbf{z}_i^E$  as  $s(\mathbf{z}_i^E, L)$ . Then the assimilation A is described as:

$$A(\mathbf{z}_i^E; \mathbf{L}) = \mathrm{GS}(\mathrm{softmax}(s(\mathrm{sg}(\mathbf{z}_i^E), \mathbf{L})))\mathbf{L},\tag{5}$$

where sg denotes the stop-grad function. The objective for learning landmarks is then  $\mathcal{L}_{MBC}(Z, A(Z^E; \mathbf{L}))$ , optimizing the consistency between the assimilated prototypes and the reference model's latent space. Landmarks are initialized as a random sample of explanation embeddings from  $Z^E$ , but then are allowed to change via gradient descent. After learning landmarks, we can measure the quality of each landmark by the number of  $\mathbf{z}_i^E$  embeddings closest to it in latent space. We filter out any landmarks that are not sufficiently close to any samples (described in Appendix B).

**TIMEX training.** The overall loss function for TIMEX has four components which we sum to produce our total loss:  $\mathcal{L} = \mathcal{L}_{MBC} + \lambda_{LC}\mathcal{L}_{LC} + \lambda_E(\mathcal{L}_m + \lambda_{con}\mathcal{L}_{con})$ , where  $\lambda_{LC}$ ,  $\lambda_E$ ,  $\lambda_{con} \in \mathbb{R}$  are weights for the label consistency loss and total explanation loss, and connective explanation loss, respectively. TIMEX can be optimized in an end-to-end fashion, and it requires little hyperparameter choices from the user. The user must also choose the r parameter for the explanation regularization. We find that explanation performance is stable across choices of r (as found in [49]), so we set r = 0.5 to remain consistent throughout experiments. A lower r value may be provided if the underlying predictive signal is known to be sparse. In total, TIMEX optimizes  $H^E$ ,  $G^E$ , and  $F^E$ .

# **5** Experimental setup

**Datasets.** We design 4 synthetic datasets with known ground-truth explanations: **FreqShapes**, **SeqComb-UV**, **SeqComb-MV**, and **LowVar**. Datasets are designed to capture diverse temporal dynamics in both univariate and multivariate settings. We employ 4 datasets from real-world time series classification tasks: **ECG** [80] - ECG arrhythmia detection; **PAM** [81] - human activity recognition; **Epilepsy** [82] - EEG seizure detection; and **Boiler** [83] - mechanical fault detection. We define ground-truth explanations for ECG as QRS intervals, which are known regions of ECG signals where arrhythmias can be detected. Such R, P, and T wave intervals are extracted following [84]. Dataset details are given in Appendix C.1 and C.4.

**Baselines.** We evaluate the method against five explainability baselines. As a general explainer, we use integrated gradients (**IG**) [31]; for recent time series-specific explainers, we use **Dynamask** [57], and **WinIT** [85]; for an explainer that uses contrastive learning, we use **CoRTX** [86]; and for an *in-hoc* explainer which has been demonstrated for time series, we use **SGT + Grad** [17].

**Evaluation.** We consider two approaches. *Ground-truth explanations:* Generated explanations are compared to ground-truth explanations, *i.e.*, known predictive signals in each input time series sample when interpreting a strong predictor, following established setups [6]. We use the area under precision (AUP) and area under recall (AUR) curves to evaluate the quality of explanations [57]. We also use the explanation AUPRC, which combines the results of AUP and AUR. For all metrics, higher values are better. Definitions of metrics are in Appendix C.4. *Feature importance under occlusion:* We occlude the bottom *p*-percentile of features as identified by the explainer and measure the change in prediction AUROC (Sec. 4.2). The most important features a strong explainer identifies should retain prediction performance under occlusion when *p* is high. To control for potential misinterpretations based on the occlusion problem, we include a random explainer reference. Our experiments use transformers [87] with time-based positional encoding. Hyperparameters, experimental, training, and compute details are given in Appendix C.

# 6 Results

#### **<u>R1</u>**: Comparison to existing methods on synthetic and real-world datasets.

**Synthetic datasets.** We compare TIMEX to existing explainers on the task of identifying important signals in time series datasets. Tables 1-2 show results for univariate and multivariate datasets, respectively. Across univariate and multivariate settings, TIMEX is the best explainer on 10/12 (3 metrics in 4 datasets) with an average improvement in the explanation AUPRC (10.01%), AUP (6.01%), and AUR (3.35%) over the strongest baselines. Specifically, TIMEX improves ground-truth explanation in terms of AUP by 3.07% on FreqShapes, 6.3% on SeqComb-UV, 8.43% on SeqComb-MV, and 6.24% on LowVar over the strongest baseline on each dataset. In all of these settings, AUR

Method	AUPRC	FreqShapes AUP	AUR	AUPRC	SeqComb-UV AUP	AUR
IG Dynamask WinIT CoRTX SGT + Grad	$ \begin{vmatrix} 0.7516 \pm 0.0032 \\ 0.2201 \pm 0.0013 \\ 0.5071 \pm 0.0021 \\ 0.6978 \pm 0.0156 \\ 0.5312 \pm 0.0019 \end{vmatrix} $	$\begin{array}{c} \underline{0.6912}{\pm} \pm 0.0028\\ \hline 0.2952 {\pm} 0.0037\\ 0.5546 {\pm} 0.0026\\ 0.4938 {\pm} 0.0004\\ 0.4138 {\pm} 0.0011 \end{array}$	$\begin{array}{c} \underline{0.5975} {\pm} 0.0020 \\ \hline 0.5037 {\pm} 0.0015 \\ 0.4557 {\pm} 0.0016 \\ 0.3261 {\pm} 0.0012 \\ 0.3931 {\pm} 0.0015 \end{array}$	$ \begin{vmatrix} 0.5760 \pm 0.0022 \\ 0.4421 \pm 0.0016 \\ 0.4568 \pm 0.0017 \\ 0.5643 \pm 0.0024 \\ 0.5731 \pm 0.0021 \end{vmatrix} $	$\begin{array}{c} 0.8157 {\pm} 0.0023 \\ \underline{0.8782} {\pm} 0.0039 \\ \overline{0.7872} {\pm} 0.0027 \\ 0.8241 {\pm} 0.0025 \\ 0.7828 {\pm} 0.0013 \end{array}$	$\begin{array}{c} \underline{0.2868}{\pm}0.0023\\ \hline 0.1029{\pm}0.0007\\ 0.2253{\pm}0.0016\\ 0.1749{\pm}0.0007\\ 0.2136{\pm}0.0008\\ \end{array}$
TIMEX	<b>0.8324</b> ±0.0034	<b>0.7219</b> ±0.0031	<b>0.6381</b> ±0.0022	<b>0.7124</b> ±0.0017	<b>0.9411</b> ±0.0006	<b>0.3380</b> ±0.0014
Ta	ble 1: Attribut	tion explanation	on performance	e on univariate	synthetic data	isets.

Method	AUPRC	SeqComb-MV AUP	AUR	AUPRC	LowVar AUP	AUR
IG Dynamask WinIT CoRTX SGT + Grad	$ \begin{array}{ c c c c c c c c c c c c c c c c c c c$	$\begin{array}{c} \underline{0.7483} {\pm} 0.0027 \\ \hline 0.5481 {\pm} 0.0053 \\ 0.7594 {\pm} 0.0024 \\ 0.5625 {\pm} 0.0006 \\ 0.4970 {\pm} 0.0005 \end{array}$	0.2581±0.0028 0.1953±0.0025 0.2077±0.0021 0.3457±0.0017 <b>0.4289</b> ±0.0018	0.8691±0.0035 0.1391±0.0012 0.1667±0.0015 0.4983±0.0014 0.3449±0.0010	$\begin{array}{c} \underline{0.4827}{\pm}0.0029\\ \hline 0.1640{\pm}0.0028\\ 0.1140{\pm}0.0022\\ 0.3281{\pm}0.0027\\ 0.2133{\pm}0.0029 \end{array}$	$\begin{array}{c} \underline{0.8165}{\pm}0.0016\\ \hline 0.2106{\pm}0.0018\\ \hline 0.3842{\pm}0.0017\\ \hline 0.4711{\pm}0.0013\\ \hline 0.3528{\pm}0.0015 \end{array}$
TIMEX	<b>0.6878</b> ±0.0021	<b>0.8326</b> ±0.0008	$0.3872 \pm 0.0015$	<b>0.8673</b> ±0.0033	<b>0.5451</b> ±0.0028	<b>0.9004</b> ±0.0024

Table 2: Attribution explanation performance on multivariate synthetic datasets.

is less important than AUP since the predictive signals have redundant information. TIMEX achieves high AUR because it is optimized to output smooth masks over time, tending to include more of entire subsequence patterns rather than sparse portions, which is an important property for human interpretation. We show TIMEX's explanations in Appendix C.5 to visualize this property.

**Real-world datasets: arrhythmia detection.** We demonstrate TIMEX on ECG arrhythmia detection. TIMEX's attribution maps show a state-of-the-art performance for finding relevant QRS intervals driving the arrhythmia diagnosis and outperform the strongest baseline by 5.39% (AUPRC) and 9.83% (AUR) (Table 3). Integrated gradients achieves a slightly higher AUP, whereas state-of-the-art time series explainers perform poorly. Notably, TIMEX's explanations are significantly better in AUR, identifying larger segments of the QRS interval rather than individual timesteps.

Ablation study on ECG data. We conduct ablations on the ECG data using TIMEX (Table 3). First, we show that the STE improves performance as opposed to soft attention masking, resulting in an AUPRC performance gain of 9.44%; this validates our claims about the pitfalls of soft masking for time series. Note that this drop in performance becomes more significant when including direct-value masking, as we show in Appendix C.6. Second, we use SimCLR loss to align  $Z^E$  to Z as opposed to MBC; SimCLR loss is able to achieve comparable results in AUPRC and AUR, but the AUP is 13.6% lower than the base TIMEX. Third, we experiment with the usefulness of MBC and LC objectives. MBC alone produces poor explanations with AUPRC at 65.8% lower score than the base model. LC alone does better than MBC alone, but its AUPRC is still 21.5% lower than the base model. MBC and LC in conjunction produce high-quality explanations, showing the value in including more intermediate states for optimizing  $G^E(H^E(\cdot))$ . Extensive ablations are provided in Appendix C.6.

# R2: Occlusion experiments on real-world datasets.

We evaluate TIMEX explanations by occluding important features from the reference model and observing changes in classification [62, 57, 86]. Given a generated explanation  $E(\mathbf{x}_i)$ , the bottom *p*-percentile of features are occluded; we expect the classification performance to drop significantly when replacing important features (identified by the explainer) with baseline values. To counter misinterpretation induced by the occlusion problem (Sec. 3.1), we compare the performance under occlusion to random explanations. We adopt the masking procedure described in Sec. 4.2, performing attention masking where applicable and direct-value masking otherwise.

Method	AUPRC	ECG AUP	AUR	TIMEX Ablations	AUPRC	ECG AUP	AUR
IG		· · · · · — · · · · ·	0.3204±0.0012			$0.5663 {\pm} 0.0025$	
Dynamask	$0.3280 \pm 0.0011$	$0.5249 \pm 0.0030$	$0.1082 \pm 0.0080$	-STE	$0.4014 \pm 0.0019$	$0.5570 {\pm} 0.0032$	$0.1564 \pm 0.0007$
WinIT	$0.3049 \pm 0.0011$	$0.4431 \pm 0.0026$	$0.3474 \pm 0.0011$	+SimCLR	$0.4767 \pm 0.0021$	$0.4895 \pm 0.0024$	$0.4779 \pm 0.0013$
CoRTX	$0.3735 \pm 0.0008$	$0.4968 \pm 0.0021$	$\overline{0.3031} \pm 0.0009$	Only LC	$0.3704 \pm 0.0018$	$0.3296 {\pm} 0.0019$	$0.5084 {\pm} 0.0008$
SGT + Grad	$0.3144 \pm 0.0010$	$0.4241 {\pm} 0.0024$	$0.2639 \pm 0.0013$	Only MBC	$0.1615 \pm 0.0006$	$0.1348 {\pm} 0.0006$	$0.5504{\pm}0.0011$
TIMEX	<b>0.4721</b> ±0.0018	$0.5663 \pm 0.0025$	0.4457±0.0018				

Table 3: (Left) Benchmarking TIMEX on the ECG dataset. (Right) Results of ablation analysis.



Figure 3: Occlusion experiments on real-world datasets. Higher values indicate better performance.



Figure 4: Landmark analysis of TIMEX on the ECG dataset. Shown is a UMAP plot of the latent explanation space along with learned landmark explanations. For two selected landmarks (in red), we show three explanation instances most similar to each landmark.

Figure 3 compares TIMEX to Dynamask, a strong time-series explainer. On all datasets, TIMEX's explanations are either at or above the performance of Dynamask, and both methods perform above the random baseline. On Boiler dataset, we demonstrate an average of 27.8% better classification AUROC across each threshold compared to Dynamask, with up to 37.4% better AUROC at the 0.75 threshold. This gap in performance between TIMEX and Dynamask is likely because the underlying predictor for Boiler is weaker than that of Epilepsy or PAM, achieving 0.834 AUROC compared to 0.979 for PAM and 0.939 for Epilepsy. We hypothesize that TIMEX outperforms Dynamask because it considers simply changes in predicted labels under perturbation while TIMEX optimizes for consistency across both labels and embedding spaces in the surrogate and reference models. TIMEX performs well across both univariate (Epilepsy) and multivariate (PAM and Boiler) datasets.

# **<u>R3:</u>** Landmark explanation analysis on ECG.

To demonstrate TIMEX's landmarks, we show how landmarks serve as summaries of diverse patterns in an ECG dataset. Figure 4 visualizes the learned landmarks in the latent space of explanations. We choose four representative landmarks based on the previously-described landmark ranking strategy (Sec. 4.4). Every landmark occupies different regions of the latent space, capturing diverse types of explanations generated by the model. We show the three nearest explanations for the top two landmarks in terms of the nearest neighbor in the latent space. Explanations (1), (2), and (3) are all similar to each other while distinctly different from (4), (5), and (6), both in terms of attribution and temporal structure. This visualization shows how landmarks can partition the latent space of explanations into interpretable temporal patterns.

# 7 Conclusion

We develop TIMEX, an interpretable surrogate model for interpreting time series models. By introducing the novel concept of model behavior consistency (*i.e.*, preserving relations in the latent space induced by the pretrained model when compared to relations in the latent space induced by TIMEX), we ensure that TIMEX mimics the behavior of a pretrained time series model, aligning influential time series signals with interpretable temporal patterns. The generation of attribution maps and the utilization of a latent space of explanations distinguish TIMEX from existing methods. Results on synthetic and real-world datasets, as well as case studies involving physiological time

series, demonstrate the superior performance of TIMEX compared to state-of-the-art interpretability methods. TIMEX's innovative components offer promising potential for training interpretable models that capture the behavior of pretrained time series models.

**Limitations.** While TIMEX is not limited to a specific task as an explainer, our experiments focus on time series classification. TIMEX can be used to explain other downstream tasks assuming we can access the latent pretrained space, meaning it could be used to examine general pretrained models for time series. However, the lack of such pretrained time series models and the lack of datasets with reliable ground-truth explanations restricted our testing in this area. One limitation of our approach is its parameter efficiency due to the separate optimization of the explanation-tuned model. Larger models may require adopting parameter-efficient tuning strategies.

# Acknowledgements

We gratefully acknowledge the support of the Under Secretary of Defense for Research and Engineering under Air Force Contract No. FA8702-15-D-0001 and awards from NIH under No. R01HD108794, Harvard Data Science Initiative, Amazon Faculty Research, Google Research Scholar Program, Bayer Early Excellence in Science, AstraZeneca Research, and Roche Alliance with Distinguished Scientists. Any opinions, findings, conclusions or recommendations expressed in this material are those of the authors and do not necessarily reflect the views of the funders. The authors declare that there are no conflict of interests.

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# Appendix A Further discussion of background

**Straight-through estimators.** Discrete operations, such as thresholding, are often avoided in neural network architectures due to difficulties differentiating discrete functions. To circumvent these issues, [75] introduce the straight-through estimator (STE), which uses a surrogate function during backpropagation to approximate the gradient for a non-differentiable operation. STEs have seen usage in quantized neural networks [S1]. This method shows empirical performance even though there is little theoretical justification behind it [S2].

**Self-supervised learning.** Methods in self-supervised learning (SSL) have become a common pretraining technique for settings in which large, unlabeled datasets are available [S3, S4, S5, S6]. Common approaches for self-supervised learning are contrastive learning, which seeks to learn representations for samples under invariant data augmentations, and metric learning, which aims to learn a latent space in which a distance function captures some pre-defined relations on data [S7]. Consistency learning has emerged as another promising SSL approach; intuitively, this family of methods seeks to learn latent spaces in which similar pairs are expected to be embedded similarly, *i.e.*, preserving some consistent properties. Consistency learning has seen use in aligning videos [S8], enhancing latent geometry for multimodal contrastive learning [78], and pretraining time series models across time and frequency domains [1].

# **Appendix B** Further theoretical discussions

# **B.1** Differentiable attention masking

As is described in Section 4.1, we use differentiable attention masking [76], which is defined as such:

$$\alpha^{m} = (\operatorname{softmax}(\frac{\mathbf{Q}\mathbf{K}^{T}}{\sqrt{d_{k}}}) \odot \mathbf{M}_{\mathcal{X}})\mathbf{V},\tag{6}$$

where  $\mathbf{Q}, \mathbf{K}, \mathbf{V}$  represent query, key and values operators,  $d_k$  is used as a normalization factor, and  $\mathbf{M}_{\mathcal{X}}$  is a mask with self-attention values. This procedure is fully differentiable, and given that  $\mathbf{M}_{\mathcal{X}}$  is binarized via the STE, it sets all attention values to zero that are to be ignored based on output from  $H^E$ .

#### **B.2** Further discussion on the utility of model behavior consistency

The model behavior consistency (MBC) framework in TIMEX is a method to train an interpretable surrogate model  $G^E$ . In Section 4.3, we discuss the conceptual advances of this approach. Here, we will outline another advantage of the approach—preserving classification performance—and a brief discussion on the broader uses of MBC in other domains and applications.

Training an *in-hoc* model is often challenging, as the inherent interpretability mechanism can hinder the performance and expressiveness of the method; this is an advantage of *post-hoc* or surrogate methods. MBC allows one to preserve the performance of the underlying predictor. TIMEX, a surrogate method, allows one to keep the predictions from a pre-trained time series encoder and develop explanations on top of it, which is practical for real-world use when a drop in classification performance is highly undesirable.

MBC is not limited to time series classification tasks. We demonstrate the utility of MBC for time series due to the particularly challenging nature of the data modality and the lack of available time series explainers. However, MBC gives a general framework for learning interpretable surrogate models through learning the  $H^E$  and  $G^E$  modules. MBC also has the potential to be applied to tasks outside of classification; since MBC is defined on the embedding space, any model with such an embedding space could be matched through a surrogate model as in TIMEX. This opens the possibility to learn on general pre-trained models or even more complex tasks such as forecasting. Finally, we see MBC as having potential beyond explainability as well; one could imagine MBC being a way to distill knowledge into smaller models [S9, S10, S11]. We leave these discussions and experiments for future work.

#### B.3 Explanation landmark selection strategy

We proceed to describe how landmarks are selected for final interpretation. As described in Section 4.4, landmarks are initialized with the embeddings given by G for a random number of training samples. Practically, we stratify this selection across classes in the training set. Landmarks are then updated during the learning procedure. After learning landmarks, not every landmark will be helpful as an explanation; thus, we perform a filtration procedure. Intuitively, this filtration consists of detecting landmarks for which the landmark is the nearest landmark neighbor for many samples. This procedure is described in Algorithm 1.

#### Algorithm 1: Landmark filtration

**Input:** Landmark matrix  $\mathbf{L} \in \mathbb{R}^{n_L \times d_z}$ ; training explanation embeddings  $\{\mathbf{z}_1^E, ..., \mathbf{z}_N^E\}$  for  $\mathbf{z}_i^E \in \mathbb{R}^{d_z}$ ; threshold number of neighbors  $n_{\epsilon} \in \mathbb{N}$   $N_l \leftarrow \{\}$ for  $i \leftarrow 1$  to N do Compute similarity to all landmarks  $S_i^l = \sin(\mathbf{z}_i^E, \mathbf{L})$   $j_{\max} \leftarrow \operatorname{argmax}_j S_i^l[j]$  (Gets nearest landmark for sample explanation i) Append  $j_{\max}$  to  $N_l$ end  $F_l \leftarrow$  Frequency of occurrence of each unique element in  $N_l$   $\mathbf{L}_{\text{filter}} \leftarrow$  every landmark in  $\mathbf{L}$  s.t.  $F_l \ge n_{\epsilon}$ Return  $\mathbf{L}_{\text{filter}}$ 

# Appendix C Additional experiments and experimental details

# C.1 Description of datasets

We conduct experiments using both synthetic and real-world datasets. This section describes each synthetic and real-world dataset, including how ground-truth explanations are generated when applicable.

# C.1.1 Synthetic datasets

We employ synthetic datasets with known ground-truth explanations to study the capability to identify the underlying predictive signal. We follow standard practices for designing synthetic datasets, including tasks that are predictive and not susceptible to shortcut learning [S12] induced by logical shortcuts. These principles are defined in [88] concerning graphs, but we extend these to synthetic datasets for time series. Each time series is initialized with a non-autoregressive moving average (NARMA) noise base, and then the described patterns are inserted. We will briefly describe the construction of each time series dataset in this section, and the codebase contains full details at https://anonymous.4open.science/r/TimeX-C1AD. We designed four synthetic datasets to test different time series dynamics:

**FreqShapes.** Predictive signal is determined by the frequency of occurrence of an anomaly signal. To construct the dataset, take two upward and downward spike shapes and two frequencies, 10 and 17 time steps. There are four classes, each with a different combination of the attributes: class 0 has a downward spike occurring every 10 time steps, class 1 has an upward spike occurring every 10 time steps, class 2 has a downward spike occurring every 17 time steps, and class 3 has an upward spike occurring every 17 time steps. Ground-truth explanations are the locations of the upward and downward spikes.

**SeqComb-UV.** Predictive signal is defined by the presence of two shapes of subsequences: increasing (I) and decreasing (D) trends. First, two subsequence regions are chosen within the time series so neither subsequence overlaps; each subsequence is 10-20 time steps long. Then, a pattern is inserted based on the class identity; the increasing or decreasing trend is created with a sinusoidal noise with a randomly-chosen wavelength. Class 0 is null, following a strategy in [88] that recommends using null classes for simple logical identification tasks in synthetic datasets. Class 1 is I, I; class 2 is D, D; and class 3 is I, D. Thus, the model is tasked with identifying both subsequences to classify each sample. Ground-truth explanations are the I and/or D sequences determining class labels.

**SeqComb-MV.** This dataset is a multivariate version of **SeqComb-UV**. The construction and class structure is equivalent, but the I and D subsequences are distributed across different sensors in the input. Upon constructing the samples, the subsequences are chosen to be on random sensors throughout the input. Ground-truth explanations are given as the predictive subsequences on their respective sensors, *i.e.*, the explainer is required to identify the time points at which the causal signal occurs and the sensors upon which they occur.

**LowVar.** Predictive signal is defined by regions of low variance over time that occur in a multivariate time series sample. Similar to **SeqComb** datasets, we choose a random subsequence in the input and, in that subsequence, replace the NARMA background sequence with Gaussian noise at a low variance. The subsequence is further discriminated by the mean of the Gaussian noise and the sensor on which the low variance sequence occurs. For class 0, the subsequence is at mean -1.5 on sensor 0; for class 1, the subsequence is at mean 1.5 on sensor 0; for class 2, the subsequence is at mean -1.5 on sensor 1; for class 3, the subsequence is at mean 1.5 on sensor 1. This task is distinctly different from other synthetic datasets, requiring recognition of a subsequence that is not anomalous from the rest of the sequence. This presents a more challenging explanation task; a simple change-point detection algorithm could not determine the explanation for this dataset.

We create 5,000 training samples, 1,000 testing samples, and 100 validation samples for each dataset. A summary of the dimensions of each dataset can be found in Table 4.

Dataset	# of Samples	Length	Dimension	Classes
FreqShapes	6,100	50	1	4
SeqComb-UV	6,100	200	1	4
SeqComb-MV	6,100	200	4	4
LowVarDetect	6,100	200	2	4

 Table 4: Synthetic Dataset Description

# C.1.2 Real-world datasets

We employ four datasets from real-world time series classification tasks: **PAM** [81] - human activity recognition; **ECG** [80] - ECG arrhythmia detection; **Epilepsy** [82] - EEG seizure detection; and **Boiler** [83] - automatic fault detection.

**PAM [81].** It measures the daily living activities of 9 subjects with three inertial measurement units. We excluded the ninth subject due to the short length of sensor readouts. We segment the continuous signals into samples with a time window of 600 and the overlapping rate of 50%. PAM initially has 18 activities of daily life. We exclude the ones associated with fewer than 500 samples, leaving us with eight activities. After modification, the PAM dataset contains 5,333 segments (samples) of sensory signals. Each sample is measured by 17 sensors and contains 600 continuous observations with a sampling frequency of 100 Hz. PAM is labeled into eight classes where each class represents an activity of daily living. PAM does not include static attributes and the samples are approximately balanced across all eight classes.

**MIT-BIH** (ECG) [80]. The MIT-BIH dataset has ECG recordings from 47 subjects recorded at the sampling rate of 360Hz. The raw dataset was then window-sliced into 92511 samples of 360 timestamps each. Two cardiologists have labeled each beat independently. Of the available annotations, we choose to use three for classification: normal reading (N), left bundle branch block beat (L), and right bundle branch block beat (R). We choose these because L and R diagnoses are known to rely on the QRS interval [S13, S14], which will then become our ground-truth explanation (see Section C.4). The Arrhythmia classification problem involves classifying each fragment of ECG recordings into different beat categories.

**Epilepsy [82].** The dataset contains single-channel EEG measurements from 500 subjects. For every subject, the brain activity was recorded for 23.6 seconds. The dataset was then divided and shuffled (to mitigate sample-subject association) into 11,500 samples of 1 second each, sampled at 178 Hz. The raw dataset features five classification labels corresponding to different states of subjects or measurement locations — eyes open, eyes closed, EEG measured in the healthy brain region, EEG measured in the tumor region, and whether the subject has a seizure episode. To emphasize the distinction between positive and negative samples, we merge the first four classes into one, and each time series sample has a binary label indicating whether an individual is experiencing a seizure. There are 11,500 EEG samples in total.

**Boiler [83].** This dataset consists of simulations of hot water heating boilers that undergo different kinds of mechanical faults. Various mechanical sensors are recorded over time to derive a time series dataset. The learning task is to detect the mechanical fault of the blowdown valve of each boiler. The dataset is particularly challenging because it includes a large dimension-to-length ratio, unlike the other datasets which contain many more time steps than sensors (Table 5).

Tuble 5. Real World Dataset Description						
Dataset	# of Samples	Length	Dimension	Classes	Task	
PAM	5,333	600	17	8	Action recognition	
MIT-BIH	92,511	360	1 or 2	5	ECG classification	
Epilepsy	11,500	178	1	2	EEG classification	
Boiler	160,719	36	20	2	Mechanical fault detection	

Table 5: Real-World Dataset Description

#### C.2 Descriptions of baseline methods

We now describe each baseline method in further detail.

**IG** [31]. Integrated gradients is a classical attribution method that utilizes the gradients of the model to form an explanation. The method compares the gradients to a baseline value and performs Riemannian integration to derive the explanation. Integrated gradients is a popular data type agnostic interpretability method [S15], but it has no inductive biases specific for time series. We use the Captum [S16] implementation of this method, including default hyperparameters such as the baseline value.

**Dynamask [57].** This explainer is built specifically for time series and uses a perturbation-based procedure to generate explanations. The method performs iterative occlusion of various input portions, learning a mask that deforms the input time series towards a carefully-determined baseline value. This method is different from TIMEX in a few key ways. First, it performs continuous masking; TIMEX performs discrete masking through STEs. Second, it measures perturbation impact on the original model  $F(G(\cdot))$ ; TIMEX trains a surrogate model  $G^E$  to learn the explanations and measure the impact of masking the input. Third, Dynamask learns the explanations iteratively for each sample; TIMEX trains the surrogate which can then output explanations in one forward pass of  $H^E$ .

**WinIT [85].** This explainer is a feature removal explainer, similar to Dynamask. WinIT measures the impact of removing features from a time series on the final prediction value. It removes the impact of certain time intervals, learning feature dependencies across time steps. WinIT uses a generative model to perform in-distribution replacement of masked-out features. WinIT improves on a previous time series explainer, FIT [62], which is a popular baseline in time series explainability literature but is excluded in our work because WinIT is more recent and improves on FIT both conceptually and empirically.

**CoRTX [86].** Contrastive real-time explainer (CoRTX) is an explainer method that utilizes contrastive learning to approximate SHAP [3] values. This method is developed for computer vision, but we implement a custom version that works with time series encoders and explanation generators. We include this method because it uses self-supervised learning to learn explanations. TIMEX also uses a self-supervised objective to learn explanations, but our method differs from CoRTX in several ways. First, CoRTX performs augmentation-based contrastive learning while we use MBC, which avoids the definition of negatives or the careful choice of augmentations specific to the data modality. Second, CoRTX fundamentally attempts to approximate SHAP values via a small number of SHAP explanations. In contrast, TIMEX includes a masking system that can produce masks without having to fine-tune a model on a set of explanations that are derived from an external method. CorRTX has close parallels to ours in using self-supervised learning but is fundamentally different from TIMEX.

**SGT + Grad [17].** Saliency-guided training (SGT), an *in-hoc* explainer, is based on a modification to the training procedure. During training, features with low gradients are masked out to "guide" the model to focus on regions that are more important for the prediction. The method is not an explainer alone but requires using another *post-hoc* explainer to derive explanations. In our experiments, we consider saliency explanations, which are recommended by the SGT authors. The authors found that this method can improve performance on time series data. For this reason, we include it as one of our baselines to demonstrate the effectiveness of TIMEX against modern *in-hoc* explainers.

Parameter	FreqShape	SeqComb-UV	SeqComb-MV	LowVarDetect	ECG
Learning rate	0.001	0.001	0.001	0.003	0.0005
Batch size	64	64	64	64	16
Weight decay	0.001	0.001	0.001	0.0001	0.0001
Scheduler?	Yes	Yes	No	No	No
Epochs	50	50	100	100	5
r	0.5	0.5	0.5	0.5	0.5
Distance norm.	No	No	No	Yes	No
$\lambda_{ m LC}$	1.0	1.0	1.0	1.0	1.0
$\lambda_E$	2.0	2.0	2.0	2.0	2.0
$\lambda_{ m con}$	2.0	2.0	2.0	2.0	2.0
au	1.0	1.0	1.0	1.0	1.0
$n_L$	50	50	50	50	50

Table 6: Training parameters for TIMEX across all ground-truth attribution experiments.

Epilepsy	PAM	Boiler
0.0001	0.002	0.0001
32	32	32
0.001	0.001	0.001
Yes	No	Yes
50	100	50
0.5	0.1	0.5
No	Yes	No
1.0	1.0	1.0
2.0	2.0	2.0
2.0	0.0	2.0
1.0	1.0	1.0
50	50	50
	0.0001 32 0.001 Yes 50 0.5 No 1.0 2.0 2.0 1.0	0.0001         0.002           32         32           0.001         0.001           0.001         0.001           Yes         No           50         100           0.5         0.1           No         Yes           1.0         1.0           2.0         2.0           2.0         0.0           1.0         1.0

Table 7: Training parameters for TIMEX across all real-world datasets used for the occlusion experiments.

#### C.3 Hyperparameter selection

We list hyperparameters for each experiment performed in this work. For the ground-truth attribution experiments (Section 6, results **R1**), the hyperparameters are listed in Table 6. The hyperparameters used for the occlusion experiment (Section 6, results **R2**) with real-world datasets is in Table 7. We also list the architecture hyperparameters for the predictors trained on each dataset in Tables 8-9.

A few abbreviations are used for hyperparameters that are not mentioned in the main text. "Weight decay" refers to an L1 regularization on the model weights; the value for weight decay is equivalent to the weight on that term in the loss function compared to the rest of the loss terms (Section 4.4). "Scheduler?" refers to using a learning rate scheduler that decreases the learning rate by a factor of 10 if a plateau occurs. We use a scheduler that delays decreasing learning rates until after 20 epochs; not every experiment utilizes the scheduler as it is based on which choice yields lower validation loss upon convergence. "Distance norm." refers to a normalization of the distances in  $\mathcal{L}_{MBC}$ ; the loss is divided by the variance of the distances on the Z embedding space.  $\tau$  is the temperature parameter used for the Gumbel-Softmax reparameterization [72], Section 4.1.  $d_h$  refers to the dimensionality of hidden layers in the transformer predictor. Finally, "Norm. embedding" refers to an architecture choice that normalizes Z when training the predictor; this is used to prevent a poor latent space when a collapse is observed via poor latent space geometry.

A few other notes on implementation and design of TIMEX: The architecture of  $H^E$  uses the same size of  $G^E$  and encoder for  $H^E$  as for the predictor on each task. The number of transformer decoder layers is fixed at 2. Please reference the codebase for more details on these hyperparameters and implementations https://anonymous.4open.science/r/TimeX-C1AD.

# C.4 Evaluation details

Following [57], we use AUP and AUR to evaluate the goodness of identification of salient attributes as a binary classification task, which is defined in C.1:

**Definition C.1** (AUP,AUR [57]). Let **Q** be a matrix in  $\{0, 1\}^{T \times d_X}$  whose elements indicate the true saliency of the inputs contained in  $\mathbf{x} \in \mathbb{R}^{T \times d_X}$ . By definition,  $Q_{t,i} = 1$  if the feature  $x_{t,i}$  is salient

Parameter	FreqShape	SeqComb-UV	SeqComb-MV	LowVarDetect	ECG
Num. layers	1	2	2	1	1
$d_h$	16	64	128	32	64
Dropout	0.1	0.25	0.25	0.25	0.1
Norm. embedding	No	No	No	Yes	Yes
Learning rate	0.001	0.001	5e-4	0.001	2e-3
Weight decay	0.1	0.01	0.001	0.01	0.001
Epochs	100	200	1000	120	500

Table 8: Training parameters for transformer predictors across all ground-truth attribution experiment datasets.

Param.	Epilepsy	PAM	Boiler
Num. layers	1	1	1
$d_h$	16	72	32
Dropout	0.1	0.25	0.25
Norm. embedding	No	No	Yes
Learning rate	0.0001	0.001	0.001
Weight decay	0.001	0.01	0.001
Epochs	300	100	500

Table 9: Training parameters for TIMEX across all real-world datasets used for the occlusion experiments.

and 0 otherwise. Let **M** be a mask in  $\{0, 1\}^{T \times d_X}$  obtained with a saliency method. Let  $\tau \in (0, 1)$  be the detection threshold for  $m_{t,i}$  to indicate that the feature  $x_{t,i}$  is salient. This allows to convert the mask into an estimator  $\hat{Q}_{t,i}(\tau)$  via:

$$\hat{Q}_{t,i}(\tau) = \begin{cases} 1 & \text{if } m_{t,i} \ge \tau \\ 0 & \text{else.} \end{cases}$$

By considering the sets of truly salient indexes and the set of indexes selected by the saliency method:

$$A = \{(t,i) \in [1:T] \times [1:d_X] \mid q_{t,i} = 1\}$$
$$\hat{A}(\tau) = \{(t,i) \in [1:T] \times [1:d_X] \mid \hat{q}_{t,i}(\tau) = 1\}$$

the precision and recall curves that map each threshold to a precision and recall score:

$$\begin{split} \mathbf{P}:(0,1) &\longrightarrow [0,1]: \tau \longmapsto \frac{|A \cap A(\tau)|}{|\hat{A}(\tau)|} \\ \mathbf{R}:(0,1) &\longrightarrow [0,1]: \tau \longmapsto \frac{|A \cap \hat{A}(\tau)|}{|A|}. \end{split}$$

The AUP and AUR scores are the area under these curves:

$$\begin{split} \mathrm{AUP} &= \int_0^1 \mathrm{P}(\tau) d\tau \\ \mathrm{AUR} &= \int_0^1 \mathrm{R}(\tau) d\tau. \end{split}$$

**Groud-truth explanations for ECG datasets.** We extract ground-truth explanations via a QRS detection strategy following [84] because an initial set of beat labels was produced by a simple slope-sensitive QRS detector, which were then given to two cardiologists, who worked on them independently. The cardiologists added additional beat labels where the detector missed beats, deleted false detections as necessary, and changed the labels for all abnormal beats. We employ Neurokit <sup>1</sup> to extract QRS complexes and also take care to ensure that the QRS is the proper explanation for each class. We consider two types of arrhythmias: left bundle branch block beat and right bundle branch block beat, to categorize our "abnormal" class. We perform the ground-truth evaluation on only the

<sup>&</sup>lt;sup>1</sup>https://github.com/neuropsychology/NeuroKit

Method	AUPRC	No STE AUP	AUR	AUPRC	STE AUP	AUR
FreqShapes	0.6695±0.0038	0.6398±0.0038	0.5454±0.0026	0.8324±0.0034	0.7219±0.0031	0.6381±0.0022
SeqComb-MV	0.5694±0.0023	<b>0.8723</b> ±0.0006	0.3229±0.0017	0.6878±0.0021	0.8326±0.0008	0.3872±0.0015
ECG	0.4014±0.0019	0.5570±0.0032	0.1564±0.0007	0.4721±0.0018	0.5663±0.0025	0.4457±0.0018

Table 10: Ablation 1: Ablation using the STE vs. no STE. "No STE" is equivalent to continuous masking, as discussed in Section 4.2.

abnormal class, as the normal class signifies negative information, which may be harder to pinpoint based on model logic.

**Statistical analysis.** We evaluate each experiment on a 5-fold cross-validation of each dataset. We then report average performance and standard error across all folds of evaluation for each experiment, which results in the error bars seen in all tables throughout this work.

#### C.5 Visualization of explanations

Figure 5 shows an example of TIMEX explainer versus IG and Dynamask. Shown is the **SeqComb-UV** dataset, which has increasing and decreasing subsequences that determine the class label. Each explainer identifies the regions driving the prediction. IG identifies very sparse portions of the predictive region, choosing only one point out of the sequences for the explanation; this is not reasonable when scaling to large and noisier datasets where the signal might not be as clear. Dynamask seems to miss some important subsequences, identifying one or two subsequences. In contrast, TIMEX identifies a larger portion of the important subsequences due to the connection loss in Equation 2. This property becomes crucial when scaling to time series datasets with more noise as it becomes more difficult to intuitively deduce the causal signal through visual inspection.

#### C.6 Further ablation experiments

We present a more in-depth study of ablations on TIMEX with respect to three datasets: FreqShapes (univariate), SeqComb-MV (multivariate), and ECG (real-world). This is an extension to the ablations on the ECG dataset in Section 6, **R1** in Table 3.

**Ablation 1: No STE.** We now conduct an experiment examining the effectiveness of using the STE for training TIMEX. Table 10 shows the results of this ablation experiment. Using the STE provides over a 17% increase in AUPRC for attribution identification for every dataset. Furthermore, AUR is better when using an STE for every dataset, but the AUP is better for SeqComb-MV without the STE than with the STE. Using the STE also shows benefits in both the univariate (FreqShapes, ECG) and multivariate (SeqComb-MV) settings. In conclusion, the STE provides a noticeable benefit over a continuous masking approach, giving empirical evidence for the claims made in Section 4.2.

**Ablation 2: SimCLR vs. MBC.** We now test a classical SimCLR [S5] contrastive learning loss against our proposed model behavior consistency (MBC). The SimCLR objective is designed to decrease the distance between explanation embeddings and embeddings in the reference model's latent space. We *do not* perform data augmentations as in the original SimCLR work. The SimCLR loss that we use is given as:

$$\mathcal{L}_{\text{SimCLR}}(Z, Z^E) = \frac{1}{N} \sum_{\mathbf{z}_i \in Z, \mathbf{z}_i^E \in Z^E} -\log \frac{\exp(D(\mathbf{z}_i, \mathbf{z}_i^E))}{\sum_{j \neq i} \exp(D(\mathbf{z}_j, \mathbf{z}_i^E))}$$
(7)

For each SimCLR trial, we fixed the number of sampled negatives at 32 and kept all other parameters equal. In addition, an early stopping strategy was performed where the stopping value was based on cosine similarity between explanation embeddings and reference sample embeddings (higher similarity is better).

SimCLR loss provides a valuable objective for training TIMEX relative to baseline explainers, but MBC optimization produces more robust explanations. SimCLR delivers a slightly better AUPRC for ECG, but its AUPRC values are below that of MBC for FreqShapes and SeqComb-MV. SimCLR loss yields explanations with consistently lower AUP; AUP is closest for SeqComb-MV with only a 3.4% drop from MBC, but it is at a 17.0% decline for FreqShapes and a 13.6% drop for ECG. It



Figure 5: Visualization of explanations on **SeqComb-UV** dataset. Each column corresponds to a unique sample. All are of Class 3, which consists of one increasing subsequence and one decreasing subsequence. The methods that generate each figure are shown for each of the rows while ground truth explanations are provided in the top row.

is important to note that in addition to increased performance, MBC loss is more computationally efficient than SimCLR loss, avoiding inference on negative samples.

Ablation 3: Effect of MBC and LC losses. We now examine the effectiveness of using both model behavior consistency (Eq. 3) (MBC) and label consistency (Eq. 4) (LC) losses. Table 12 shows that using LC and MBC in combination is always better than using either one alone. In isolation, LC performs better than MBC, which is expected given its (obviously) higher correlation with the classification predictions than MBC, which relies on an earlier embedding space. Using both losses results in a powerful explainer that achieves over 27.5% higher AUPRC than MBC or LC alone. MBC and LC work together to capture rich information about the model's behavior, allowing TIMEX to be a state-of-the-art explainer.

Method	AUPRC	SimCLR AUP	AUR	AUPRC	MBC AUP	AUR
FreqShapes	0.7014±0.0046	0.5991±0.5915	0.5915±0.0027	0.8324±0.0034	0.7219±0.0031	0.6381±0.0022
SeqComb-MV	0.6645±0.0019	0.8148±0.0009	0.3777±0.0017	0.6878±0.0021	0.8326±0.0008	0.3872±0.0015
ECG	0.4767±0.0021	0.4895±0.0024	<b>0.4779</b> ±0.0013	0.4721±0.0018	0.5663±0.0025	0.4457±0.0018

Table 11: Ablation 2: Ablation considering SimCLR objective for training TIMEX versus an MBC objective as outlined in the main text.

Dataset	Ablation	AUPRC	AUP	AUR
FreqShapes	MBC only LC only MBC + LC	0.2316±0.0020 0.2629±0.0022 <b>0.8324</b> ±0.0034	0.1533±0.0015 0.1850±0.0016 <b>0.7219</b> ±0.0031	$\begin{array}{c} 0.4763 {\pm} 0.0022 \\ 0.5893 {\pm} 0.0018 \\ \textbf{0.6381} {\pm} 0.0022 \end{array}$
SeqComb-MV	MBC only	0.0761±0.0008	0.0576±0.0006	0.4996±0.0019
	LC only	0.0788±0.0009	0.0570±0.0006	<b>0.5294</b> ±0.0034
	MBC + LC	0.6878±0.0021	<b>0.8326</b> ±0.0008	0.3872±0.0015
ECG	MBC only	0.1615±0.0006	0.1348±0.0006	0.5504±0.0011
	LC only	0.3704±0.0018	0.3296±0.0019	0.5084±0.0008
	MBC + LC	<b>0.4721</b> ±0.0018	0. <b>5663</b> ±0.0025	0.4457±0.0018

Table 12: Ablation 3: Effects of model behavior consistency (MBC) and label consistency (LC) losses on explanation performance.

# C.7 Implementation and computing resources

**Implementation.** We implemented all methods in this study using Python 3.8+ and PyTorch 2.0. In our experiments, we employed the Vanilla Transformer [87] as the classification model for all methods. To ensure strong underlying predictors for explainability evaluation, as suggested by Faber et al. [88], we verified that the classification models achieved satisfactory performance on the testing set. Complete classification results are in Table 13. We followed the hyperparameters recommended by the respective authors for all baseline methods.

**Computational resources.** For computational resources, we use a GPU cluster with various GPUs, ranging from 32GB Tesla V100s GPU to 48GB RTX8000 GPU. TIMEX, and all models were only trained on a single GPU at any given time. The average experiment runtime in this work was around 5 minutes per fold, with ECG taking the longest at approximately 13 minutes per fold when training TIMEX to convergence.

# C.8 Flexible use of TIMEX with different time series architectures

We now study the ability of TIMEX to work with different underlying time series architectures. This means that of the original architecture, G and  $G^E$  are now an alternative architecture, while  $H^E$  remains as described in Section 4.1. Since experiments in the main text are based on transformer architectures, we now use a convolutional neural network (CNN) and long-short term memory (LSTM) network as the underlying predictors with the following hyperparameters:

• LSTM: 3 layer bidirectional LSTM + MLP on mean of last hidden states

Dataset	F1	AUPRC	AUROC
FreqShapes SeqComb-UV SeqComb-MV LowVar	$\begin{array}{c} 0.9716 {\pm} 0.0034 \\ 0.9415 {\pm} 0.0052 \\ 0.9765 {\pm} 0.0024 \\ 0.9748 {\pm} 0.0056 \end{array}$	$\begin{array}{c} 0.9940 {\pm} 0.0008 \\ 0.9798 {\pm} 0.0028 \\ 0.9971 {\pm} 0.0005 \\ 0.9967 {\pm} 0.0013 \end{array}$	$\begin{array}{c} 0.9980 {\pm} 0.0003 \\ 0.9921 {\pm} 0.0011 \\ 0.9990 {\pm} 0.0001 \\ 0.9988 {\pm} 0.0005 \end{array}$
Boiler ECG Epilepsy PAM	$\begin{array}{c} 0.8345 {\pm} 0.0089 \\ 0.9154 {\pm} 0.0134 \\ 0.9201 {\pm} 0.0079 \\ 0.8845 {\pm} 0.0051 \end{array}$	$0.8344 \pm 0.0071$ $0.9341 \pm 0.0169$ $0.9246 \pm 0.0130$ $0.9251 \pm 0.0029$	$\begin{array}{c} 0.8865 {\pm} 0.0159 \\ 0.9587 {\pm} 0.0111 \\ 0.9391 {\pm} 0.0157 \\ 0.9786 {\pm} 0.0009 \end{array}$

Table 13: Classification (*i.e.*, predictive) performance achieved by transformer time series models on datasets used in this study. These models are considered as time series predictors throughout experiments in this study.

Method	AUPRC	FreqShapes AUP	AUR	AUPRC	SeqComb-MV AUP	AUR
IG Dynamask WinIT	0.9282±0.0016 0.2290±0.0012 0.4171±0.0016	$\begin{array}{c} 0.7775 {\pm} 0.0010 \\ 0.3422 {\pm} 0.0037 \\ 0.5106 {\pm} 0.0026 \end{array}$	$\begin{array}{c} 0.6926 {\pm} 0.0017 \\ 0.5170 {\pm} 0.0013 \\ 0.3909 {\pm} 0.0017 \end{array}$	0.2369±0.0020 0.2836±0.0021 <b>0.3515</b> ±0.0014	0.5150±0.0048 0.6369±0.0047 <b>0.6547</b> ±0.0026	0.3211±0.0032 0.1816±0.0015 0.3423±0.0021
Ours	<b>0.9974</b> ±0.0002	<b>0.7964</b> ±0.0009	<b>0.8313</b> ±0.0011	$0.1298 {\pm} 0.0017$	$0.1307 {\pm} 0.0022$	<b>0.4751</b> ±0.0015

Table 14: Explainer results with LSTM predictor on FreqShapes and SeqComb-MV synthetic datasets.

Method	AUPRC	ECG AUP	AUR
IG Dynamask WinIT	0.5037±0.0018 0.3730±0.0012 0.3628±0.0013	$\begin{array}{c} 0.6129 {\pm} 0.0026 \\ 0.6299 {\pm} 0.0030 \\ 0.3805 {\pm} 0.0022 \end{array}$	0.4026±0.0015 0.1102±0.0007 0.4055±0.0009
Ours	<b>0.6057</b> ±0.0018	<b>0.6416</b> ±0.0024	<b>0.4436</b> ±0.0017

Table 15: Explainer results with LSTM predictor on ECG dataset.

# • CNN: 3 layer CNN + MLP on meanpool

Tables 16 17 show the results of TIMEX against strong baselines with a CNN predictor. TIMEX retains the state-of-the-art prediction observed for the transformer-based architecture, achieving the best AUPRC on SeqComb-MV and ECG datasets. However, the performance for FreqShapes saturates at very high values for both TIMEX and IG, making the comparison more difficult for AUPRC. Tables 14,15 show the results of TIMEX against strong baselines with an LSTM predictor. TIMEX performs very well for both FreqShapes and ECG datasets, achieving the highest AUPRC, AUP, and AUR for both datasets. For SeqComb-MV, TIMEX did not converge. However, no explainer performed well for this task, achieving lower results than for the transformer and CNN predictors.

Method	AUPRC	FreqShapes AUP	AUR	AUPRC	SeqComb-MV AUP	AUR
IG Dynamask WinIT	0.9955±0.0005 0.2574±0.0008 0.5321±0.0018	0.8754±0.0008 0.4432±0.0032 0.6020±0.0025	0.7240±0.0015 0.5257±0.0015 0.3966±0.0017	0.5979±0.0027 0.4550±0.0016 0.5334±0.0011	<b>0.8858</b> ±0.0014 0.7308±0.0025 0.8324±0.0020	$\substack{0.2294 \pm 0.0013 \\ 0.3135 \pm 0.0019 \\ 0.2259 \pm 0.0020}$
Ours	0.9941±0.0002	$0.6915 {\pm} 0.0010$	0.8522±0.0009	0.7016±0.0019	$0.7670 {\pm} 0.0012$	<b>0.4689</b> ±0.0016

Table 16: Explainer results with CNN predictor on FreqShapes and SeqComb-MV synthetic datasets.

	ECG			
Method	AUPRC	AUP	AUR	
IG	$0.4949 \pm 0.0010$	$0.5374 {\pm} 0.0012$	0.5306±0.0010	
Dynamask	$0.4598 {\pm} 0.0010$	$0.7216 {\pm} 0.0027$	$0.1314 \pm 0.0008$	
WinIT	$0.3963 \pm 0.0011$	$0.3292 {\pm} 0.0020$	$0.3518 \pm 0.0012$	
Ours	0.7844±0.0014	0.8706±0.0012	$0.3972 \pm 0.0010$	

Table 17: Explainer results with CNN predictor on ECG dataset.

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